Effect of radiotherapy on resin composite adaptation to the cavity wall and elastic modulus of dentin

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Purpose: This study aimed to evaluate the effects of 60 Gy γ-ray irradiation on the adaptation of resin composite restorations using two-step and one-step self-etching systems.

Materials and Methods: One-half of bovine incisors were irradiated with 60 Gy γ-ray. Flat dentin surfaces were prepared on labial side. Cylindrical cavities were prepared on flat dentin surfaces. Cavities were restored with a two-step self-etching system Clearfil SE Bond or a one-step self-etching system Clearfil tri-S Bond adhesive, followed by Clearfil AP-X composite. The composites were light-cured with 600 mW/cm² for 40 s. One-half of the specimens were thermocycled for 5,000 cycles. Dye penetration tests around the restorations were performed.

Results: Irradiation with 60 Gy γ-ray significantly decreased resin composite adaptation for the non-thermocycled Clearfil SE Bond (p < 0.05). Clearfil tri-S Bond showed significantly decreased cavity wall adaptation compared with Clearfil SE Bond, regardless of the number of thermal cycling and γ-ray irradiation (p < 0.05). Irradiation with 60 Gy γ-ray significantly decreased nanohardness and elastic modulus of the dentin (p < 0.05).

Conclusion: Irradiation with 60 Gy γ-ray significantly decreased resin composite adaptation for the non-thermocycled Clearfil SE bond. Further, nanohardness and elastic modulus of the dentin significantly decreased after the irradiation.

Key Words: adaptation, dye penetration, elastic modulus, γ-ray irradiation, microhardness, resin composite

Introduction

The aging population in society has witnessed increased incidence of tooth wear and cancer. Patients with head and neck cancer require radiotherapy in these areas [1]. Orofacial tissues, including the salivary glands, mucous membranes, taste buds, bone, and teeth are affected by radiation [2-4]. Radiation caries can be attributed to head or neck radiotherapy [5] in the cervical area of the tooth [6]. Tooth wear and radiation caries cannot be treated using metal inlays commonly used for conventional Black’s cavities. They can only be restored with resin composites using a direct bonding technique to conserve the tooth structure.

Radiation causes decrease in the saliva production resulting from salivary gland lesion [7] and changes in the microbial flora [8]. Most orofacial complications are dependent on radiation dose, and severe side-effects occur when doses are greater than 45 Gy [9]. Irradiation of 60 Gy γ-ray is the total absorbed dose in one course of radiotherapy in patients with head or neck cancer. Irradiation by 60 Gy γ-ray significantly decreased the ultimate tensile strength [10] and microhardness of the dentin [11]; however, 60 Gy γ-ray significantly increased the microhardness of superficial enamel [11]. Irradiation with 70 Gy γ-ray significantly decreased the shear bond strength of the bovine dentinoenamel junction and could cause some damage to the biophysical properties [12].

Resin composite restoration with a direct bonding technique has been indicated in cancer patients before or after irradiation. However, resin composite adaptation to the irradiated tooth substrate has seldom been reported. The effect of γ-ray irradiation on dentin remains unclear. It is hypothesized that 60 Gy γ-ray irradiation will decrease resin composite adaptation to the dentin cavity wall, dentin nanohardness, and elastic modulus.
**Materials and Methods**

**Specimen preparation**

The materials, components, manufacturers, batch numbers, and bonding procedures used in this study are listed in Table 1. An experimental quartz-tungsten halogen light-curing unit (GC, Tokyo, Japan) connected to a slide regulator (Type SD-135, Matsunaga Mfg., Yokohama, Japan) was used in this study. This light-curing unit included a control system for lamp voltage and adjustable light intensity, which was measured using a curing radiometer (model 100, Demetron Research, Danbury, CT, USA). Forty erupted intact bovine lower incisors, stored frozen after extraction, were employed in this study. One-half of the bovine incisors were irradiated with 60 Gy γ-rays using a cobalt 60 therapeutic machine (RCR-120; Toshiba, Tokyo, Japan). The labial enamel was ground using a model trimmer under running water to expose a superficial flat dentin surface and finished with a wet 600-grit SiC paper. Cylindrical cavities of 1.5 mm depth, 3 mm diameter, and a C-factor of 3 were prepared on the flat dentin surfaces of each tooth using a diamond point (#CR30, ISO No. 068 030, GC) under copious air–water spray. Each of the nine cavities was treated with a two-step self-etching system Clearfil SE Bond (SE, Kuraray Noritake Dental, Tokyo, Japan) or a one-step self-etching system Clearfil tri-S Bond (TS, Kuraray Noritake Dental). After the adhesive was cured, the cavities were bulk-filled with Clearfil AP-X resin composite (shade A3, Kuraray Noritake Dental). The resin composite was light-cured with an intensity of 600 mW/cm² for 40 s.

**Table 1** Study materials

<table>
<thead>
<tr>
<th>Material/Manufacturer</th>
<th>Componentsa</th>
<th>Batch No.</th>
<th>Bonding Instructionb</th>
</tr>
</thead>
<tbody>
<tr>
<td>Clearfil SE Bond</td>
<td>Primer: MDP, HEMA, hydrophilic aliphatic dimethacrylates, colloidal silica, photoinitiator, accelerators, water Bond: MDP, HEMA, Bis-GMA, hydrophobic aliphatic methacrylate, microfiller (colloidal silica), photoinitiator, initiator, accelerators, others</td>
<td>00761A</td>
<td>a (20 s), b, c, d, e (10 s)</td>
</tr>
<tr>
<td>Clearfil tri-S Bond</td>
<td>Bond: MDP, HEMA, Bis-GMA, photoinitiator, water, ethanol, silanated colloidal silica</td>
<td>00083A</td>
<td>c (20 s), b, e (10 s)</td>
</tr>
<tr>
<td>Clearfil AP-X, shade A3</td>
<td>silanated barium glass filler, silanated silica filler, silanated colloidal silica, Bis-GMA, TEGDMA, photoinitiator, catalyst, accelerator, pigments, others Filler load: 84.5 wt%</td>
<td>01151A</td>
<td></td>
</tr>
</tbody>
</table>

a Abbreviations: Bis-GMA, bisphenol A-glycidyl methacrylate; MDP, 10-methacryloyloxydecyl dihydrogen phosphate; HEMA, 2-hydroxyethylmethacrylate; TEGDMA, triethylene glycol dimethacrylate

b Procedures: a, apply primer; b, dry with gently air-blowing; c, apply adhesive; d, gently air-blow; e, light-cure

**Evaluation of marginal sealing and cavity wall adaptation**

After completion of light curing, the specimens were stored in the dark for 24 h in water maintained at 37°C. One-half of the specimens were subsequently thermocycled for 5,000 cycles between at 5°C and 55°C with a 30 s dwell time. The dye penetration test was used to determine the degree of adaptation to the cavity margins and walls. The test was performed by placing a 1.0% acid red propylene glycol solution (Caries Detector, Kuraray Noritake Dental) at the margin of restoration for 5 s, followed by rinsing with water and gentle blow-drying. The extent of dye penetration was observed with a stereo-microscope (20× magnification). A photographic record of each specimen was acquired at this stage.

The specimens were then longitudinally cut in half using a diamond saw microtome (77 model, Bronwill
Scientific, Rochester, NY, USA) under running water, the dye was reapplied to the sections, and images were acquired to observe the gaps. In these images, the length of dye penetration along the cavity margins and walls was measured using a digitizer (KD 4300 model, Graphtec, Tokyo, Japan). The degree of marginal leakage was defined as the length of dye penetration, which was measured as a percent of the total length of the cavity margin. Dye penetration along the cavity walls was calculated as a percent of the total cavity wall length. This was referred to as the cavity-wall gap formation. The dye penetration test scores were compared using the Kruskal-Wallis and Mann-Whitney U tests at a significance level of 5%.

**Nanohardness and elastic modulus**

Each of four teeth that were irradiated and non-irradiated were embedded using epoxy resin. The labial enamel was ground using a model trimmer under running water to expose the superficial flat dentin surface and finished with a wet diamond paste. Nanohardness and complex Young’s modulus were measured at the dentin surface of each non-irradiated and irradiated specimen. Each specimen of four nanohardness and elastic modulus were measured using a nanoindentation tester (ENT-1100, Elionix, Hachioji, Japan) with a load of 0.049 N and 12 s dwell time. Nanohardness and elastic modulus results were analyzed using the Bonferroni/Dunn test at a significance level of 5%.

**Results**

The results of marginal leakage and cavity-wall gap formation are shown in Table 2. The group of Clearfil SE Bond with 0 cycle showed no dye penetration on margin, regardless of γ-ray irradiation. γ-ray irradiation significantly decreased the resin composite adaptation to the cavity wall of Clearfil SE Bond with 0 cycle group ($p < 0.05$). There was no significant difference between the irradiated and non-irradiated groups with 5,000 cycles thermal cycling on marginal sealing and cavity wall adaptation for Clearfil SE Bond ($p > 0.05$). However, 5,000 cycles thermal cycling significantly increased resin composite adaptation to the cavity wall compared with the group of 0 cycle thermal cycling of the γ-ray irradiated for Clearfil SE Bond ($p < 0.05$).

<table>
<thead>
<tr>
<th>Number of thermal cycling</th>
<th>Adhesive system</th>
<th>Marginal leakage (%)</th>
<th>Cavity-wall gap formation (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td></td>
<td>Non-irradiated</td>
<td>Irradiated</td>
</tr>
<tr>
<td>0</td>
<td>SE</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td></td>
<td>TS</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>5,000</td>
<td>SE</td>
<td>1.1 (3.2)</td>
<td>0.9 (2.9)</td>
</tr>
<tr>
<td></td>
<td>TS</td>
<td>1.1 (3.2)</td>
<td>0.7 (2.2)</td>
</tr>
</tbody>
</table>

Intergroup data designated with the same lower-case superscript letters for each non-irradiated or irradiated dentin substrate are significantly different ($p < 0.05$). Intergroup data designated with the same upper-case superscript letters for each thermal cycling number are significantly different ($p < 0.05$). SD in parentheses, Intragroup data connected by a vertical line for adhesive type are significantly different ($p < 0.05$).

The group of Clearfil tri-S Bond with 0 cycle group showed no dye penetration on margin, regardless of γ-ray irradiation. There was no significant difference between the irradiated and non-irradiated groups with 5,000 cycles thermal cycling on marginal sealing and cavity wall adaptation for Clearfil tri-S Bond ($p > 0.05$). Clearfil tri-S Bond significantly decreased resin composite adaptation to the cavity wall compared with Clearfil SE Bond, regardless of γ-ray irradiation and thermal cycling number ($p < 0.05$).

There was no significant difference between 0 cycle and 5,000 cycles on marginal sealing of the
non-irradiated group for both Clearfil SE Bond and Clearfil tri-S Bond ($p > 0.05$). However, thermal cycling at 5,000 cycles significantly increased resin composite adaptation to the cavity wall compared with the irradiated group with 0 cycle for both Clearfil SE Bond and Clearfil tri-S Bond ($p < 0.05$).

The results of nanohardness and elastic modulus of dentin are shown in Table 3. Nanohardness and elastic modulus of the irradiated dentin were significantly lower than that of non-irradiated dentin ($p < 0.05$).

### Table 3 Nanohardness and elastic modulus of non-irradiated and γ-ray irradiated dentin

<table>
<thead>
<tr>
<th></th>
<th>Nanohardness (GPa)</th>
<th>Elastic Modulus (GPa)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Non-irradiated</td>
<td>0.56 (0.02)</td>
<td>25.9 (1.3)</td>
</tr>
<tr>
<td>Irradiated</td>
<td>0.53 (0.05)</td>
<td>21.4 (3.2)</td>
</tr>
</tbody>
</table>

Intragroup data connected by a vertical line are significantly different ($p < 0.05$). SD in parentheses

**Discussion**

Irradiation with 60 Gy γ-ray significantly decreased the resin composite adaptation to the cavity wall compared with non-irradiation for Clearfil SE Bond of non-thermal cycling group. Irradiation with 60 Gy γ-ray significantly decreased nanohardness and elastic modulus of the irradiated dentin compared with the non-irradiated dentin. This finding supported previous report that 60 Gy γ-ray significantly reduced Knoop hardness of the human dentin [11]. Yoshikawa et al. have already reported that 60 Gy γ-ray irradiation showed some effect to dentin morphology [13]. It was reported that 60 Gy γ-ray irradiation significantly decreased the ultimate tensile strength [10], and shear bond strength of resin composite to the dentin [14]. Moreover, 60 Gy γ-ray [11,13] or 70 Gy γ-ray [12] irradiation caused some damage to the dentin collagen. Therefore, 60 Gy γ-ray irradiation decreased resin composite adaptation to the cavity wall for Clearfil SE Bond.

Thermal cycling at 5,000 cycles significantly increased resin composite adaptation to the cavity wall compared with the irradiated group with 0 cycle for both two-step self-etching system Clearfil SE Bond and one-step self-etching system Clearfil SE Bond. It was reported that resin composite bond strength to dentin of 1 min after light curing was lower than that of 24 h after light curing [15]. Therefore, thermal cycling increased composite adaptation to the cavity wall for irradiated group because of accelerated adhesive polymerization. It is thought that bond strength of both one-step and two-step self-etching systems were affected by γ-ray irradiation damage to the dentin at the early stage of bonding.

The two-step self-etching system Clearfil SE Bond showed excellent resin composite adaptation to the dentin cavity wall. However, one-step self-etching system Clearfil tri-S Bond showed significantly decreased resin composite adaptation to the dentin cavity wall compared with two-step self-etching system Clearfil SE Bond regardless of γ-ray irradiation and thermal cycling number. The mechanical properties of each component of resin–dentin bond complex (resin composite, adhesive layer, hybrid layer, and underlying dentin), are believed to play significant roles in bond stability that may contribute to bond durability [16,17]. It was reported that Clearfil SE Bond had significantly less water sorption compared with other adhesives [18]. During the thermal cycling procedure, the specimens were subjected to temperature changes and water immersion. Lower water sorption, hence less water molecules within the polymer matrix, helped to maintain the mechanical properties of dental resins over time. Thus, this lower water sorption behavior may account for the more durable bond [19,20]. Moreover, Yoshikawa et al. have already reported that the two-step self-etching system Clearfil SE Bond showed high microtensile bond strength on deep flat (thin RDT) dentin [21] and on Class I dentin cavity floor.
and wall as compared with one-step self-etching system Clearfil tri-S Bond [22,23]. Thus, Clearfil SE Bond showed excellent resin composite adaptation to the dentin cavity wall.

Conversely, one-step self-etching systems are more hydrophilic and water absorbent than two-step systems [18]. This water sorption plasticize polymers and increases solubility while decreasing the modulus of elasticity and the mechanical properties of the polymers [24]. Therefore, the one-step self-etching system Clearfil tri-S Bond showed lower adaptation to the cavity wall.

It was reported that 60 Gy γ-ray irradiation showed no effect on the resin composite tensile bond strengths for the human flat dentin with four different dentin bonding agents using divided irradiation for 6 weeks [25]. Further research is required to confirm the clinically divided γ-ray irradiation effect of resin composite adaptation and bonding to the tooth substrate.

Irradiation with 60 Gy γ-ray significantly decreased resin composite adaptation for the non-thermocycled Clearfil SE bond. Further, nanohardness and elastic modulus of the dentin significantly decreased after the irradiation.

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Conflict of Interest
There are no conflicts of interest to declare.

References

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